IN THE SPECIFICATION:

Page 9, please amend the paragraph beginning at lines 5 and 13 as follows:

~~FIG. 7 is a view~~ FIGS. 7A, 7B and 7C are used to describe an example of settings of selection conditions of residual images stored in attenuation tables 1 through 4 for the continuous radiography of FIG. 6.

As is shown in FIG. 1, an X-ray image diagnostic apparatus comprises an X-ray source 3, such as an X-ray tube, that generates X-rays, an X-ray flat panel detector 4 placed oppositely to the X-ray source ~~4~~ 3, a C-arm 5 that supports the X-ray source ~~4~~ 3 and the X-ray flat panel detector 3, a leg portion 6 that holds the C-arm 5 to stand on the floor, an X-ray generation high-voltage power source 7 that is electrically connected to the X-ray source ~~4~~ 3, an image processing portion 8 that is electrically connected to the X-ray flat panel detector 3, and an image display portion (monitor) 9 that is electrically connected to the image processing portion 8.

Page 19, please amend the paragraph beginning at line 17 as follows:

Operations of the X-ray image diagnostic apparatus of the third embodiment will now be described. When the 2 × 2 read fluoroscopic mode is carried out after an exposure, the control portion ~~11~~ 13 controls the multiplexer 15a in such a manner that an output from the image memory 10 is inputted to the attenuation table 11d for the 2 × 2 read fluoroscopic mode. Correction means same as in the first embodiment is thus applied to an image in the 2 × 2 read fluoroscopic mode. Likewise, when the 1 × 1 read fluoroscopic mode is carried out, the control portion 13 controls the multiplexer 15a in such a manner that an output from the image memory 10 is inputted to the attenuation table 11c for 1 × 1. Correction means same as in the first embodiment is thus applied to an image in the 1 × 1 read fluoroscopic mode. Incidentally, when the read pixel size is changed during fluoroscopy, conversion is necessary because an image recorded in the image memory 10 and a fluoroscopic

image that needs correction are of different sizes. When the 2 × 2 read fluoroscopic mode is carried out before an exposure, residual image data in the 2 × 2 read fluoroscopic mode is recorded in the image memory 10. Likewise, when the 1 × 1 read fluoroscopic mode is carried out, residual image data in the 1 × 1 read fluoroscopic mode is recorded in the image memory 10. Normally, fast processing is required for a fluoroscopic image, and an input to the image processing portion 8 is handled in a size of the 2 × 2 read fluoroscopic mode. The image memory 10 therefore has a recording size of the 2 × 2 read fluoroscopic mode, too. In this case, when the fast fluoroscopic mode is switched to the high-definition fluoroscopic mode, the 2 × 2 read fluoroscopic mode is carried out before an exposure, and the 2 × 2 read fluoroscopic mode is changed to the 1 × 1 fluoroscopic mode after the exposure. Of the residual image data recorded in the image memory 10, data of an image region in the 1 × 1 read fluoroscopic mode is sent to the attention table 11c for the 1 × 1 read fluoroscopic mode. This is because when data of the image region alone is sent, high definition is maintained and yet a rate of processing speed can be taken into account by optimizing a data volume. In this instance, a single pixel in the residual image data in the 2 × 2 read fluoroscopic mode stored in the image memory 10 is inputted to four pixels at positions corresponding to this pixel in the residual image data in the 1 × 1 read fluoroscopic mode within the attenuation table ~~12~~ 11c. Also, the 1 × 1 read fluoroscopic mode is carried out before an exposure, and 1 × 1 exposure is carried out subsequently. Further, when the 1 × 1 read fluoroscopic mode is changed to the 2 × 2 read fluoroscopic mode after this exposure, neighboring four pixels within the ~~record~~ image memory 10 are averaged before being input to the attenuation table, and then outputted to the 2 × 2 attenuation table 11d.

Please delete pages 32-35 in their entirety.